



Minimizing Invasiveness in Neurosurgical Osteotomies: A Comparative Histomorphometric Study of Piezoelectric Craniotomy versus High-Speed Drill

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■ **BACKGROUND:** Piezoelectric bone cutting has gained popularity in neurosurgical osteotomies due to perceived lower trauma compared to rotary instruments. However, histological confirmation of its decreased aggressiveness is lacking, hindering conclusive proof. This study compares the bony and neuro-meningeal invasiveness of piezoelectric craniotomy with high-speed drill techniques.

■ **METHODS:** Histological data from 21 sheep undergoing piezoelectric craniotomy and 19 sheep subjected to high-speed electric drill craniotomy were compared. Piezoelectric craniotomy utilized a 0.35 mm micro saw titanium nitride coated. Outcome parameters included the detection of the "smear layer," average osteoblast count per high-power field, and residual bone matrix for bony invasiveness assessment. Parameters for meningeal and brain parenchymal invasiveness included pachymeningeal and leptomeningeal injury, gliosis, and histiocytic infiltration. Statistical significance was determined at $P < 0.05$.

■ **RESULTS:** Results showed the Piezo group had fewer frequent smear layers ($P < 0.001$), higher residual bone matrix ($P < 0.05$), and greater osteoblast counts per high-power field ($P < 0.05$). Additionally, the Piezo group exhibited lower rates of leptomeningeal injury, cerebral gliosis, and histiocytic infiltration ($P < 0.05$).

■ **CONCLUSIONS:** Piezoelectric craniotomy preserves residual osteoblast viability and leptomeningeal integrity

while demonstrating lower rates of thermally induced gliosis and histiocytic infiltration compared to high-speed drills. This suggests the piezoelectric osteotome's minimal invasiveness in bone, meningeal, and brain tissue.

INTRODUCTION

Piezoelectric bone cutting is the result of the combination between the mechanical effect of ultrasound and the physical phenomenon of cavitation, the latter enhancing the former.^{1,2} The phenomenon of cavitation leads to the formation of vapor-filled cavities as a result of abrupt and rapid pressure changes in a fluid.³ These cavities collapse under the impact of a high-pressure change, creating a high-energy shock wave that propagates through the biological tissue, including the mineralized tissue.^{1,3} As a result of the shock wave propagation, the biomechanical adhesion between the cell layer and the substrate is weakened, facilitating mechanical cutting of the tissue. In piezoelectric surgery, the source of pressure changes at the base of cavitation are the piezoelectric crystals, which can deform when exposed to an electric field that falls in the ultrasonic frequency spectrum.^{4,5} These concepts constitute the physical basis of the so-called "indirect piezo effect."^{6,7} The linear micrometric (60–210 μm) vibrations, when delivered at an oscillation frequency ranging between 25 and 30 kHz, are responsible for the selectivity of the piezoelectric cut on the

Key words

- Bone healing
- Gliosis
- High-speed drills
- Histomorphometric study
- Neurosurgical osteotomies
- Piezoelectric craniotomy
- Thermal damage

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Supplementary digital content available online.

Citation: *World Neurosurg.* (2024) 191:e160-e166.
<https://doi.org/10.1016/j.wneu.2024.08.088>

Journal homepage: www.journals.elsevier.com/world-neurosurgery

Available online: www.sciencedirect.com

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mineralized bone while sparing the underlying and neighboring soft tissues and neurovascular structures.^{2,4}

In addition, the irrigation system coupled with the instrument leads to the avoidance of thermal injury. All these technical characteristics make the piezoelectric bone scalpel theoretically superior to the conventional rotary osteotomes used in neurosurgery, oto-neurosurgery, and maxillo-facial surgery. In confirmation of this, several studies have already been reported in the literature.⁸⁻²⁹ However, very few of them aimed at histologic confirmation of the presumed less aggressiveness of piezo surgery compared to rotary instruments. The same applies to the dynamics of bone healing in relation to the viability of residual osteoblasts.

The aim of the present study was to analyze the invasiveness of piezoelectric craniotomy from a histomorphometric point of view. A comparative evaluation with the high-speed drill was also performed.

METHODS

The *in vivo* study was conducted at the Dipartimento di Medicina di Precisione e Rigenerativa Area Jonica facility, University of Bari, Italy, with Ministry of Health protocol approval (#654/2020).

Histological data of cranial vault, meningeal, and cerebral parenchymal samples from 21 sheep that underwent craniotomy with a piezoelectric bone scalpel (Mectron Piezosurgery Touch, Mectron Medical Technology, Genoa, Italy) (Figure 1) (Piezo group) were collected and compared with those from 19 sheep that underwent craniotomy with a high-speed electric drill (Osseoduo, Bien-Air Surgery, Biel, Switzerland)

(speed range: 0–80,000 rpm, torque: 4.5 N/cm) (control group). A specially designed micro saw of 0.35 mm titanium nitride coated (OT12, Osteotomy Tips Kit, Mectron Medical Technology, Genoa, Italy) (Figure 1C) was mounted on the piezoelectric scalpel handpiece (Figure 1D). The micro saw has 3 landmarks (Figure 1C, black dots) indicating depths of 7, 8.50, and 10 mm. This characteristic, together with the elongated shape of the micro saw, allowed for deeper cuts. A preset power on the Piezosurgery touch screen of 16 W, designated for cortical bone, was applied with 25–30 KHz frequency modulation and 60–120 μ m linear microvibrations. The irrigation rate was 30 mL/min. Figure 2 illustrates the key operative steps of a piezoelectric craniotomy.

In the control group, the handpiece was equipped with an irrigation nozzle connected to a peristaltic pump, and the saline flow was set at 80%. During surgery, the flow was increased to 100% on a case-by-case basis, depending on the need for greater cooling and/or clearer vision of the surgical field. Only 6.0 mm right fluted burrs were used.

Video 1 shows a comparison between piezoelectric and high-speed drill craniotomies.

Cranial vault and pachymeningal specimens were harvested en bloc, as were the leptomeninges and underlying cerebral parenchyma. Histological studies were performed by hematoxylin-eosin staining.



Outcome Measures

The detection of “smear layer,”³⁰⁻³³ mean number of osteoblasts/high-power field, and bone matrix were considered as outcome parameters of the invasiveness of the technique to the adjacent

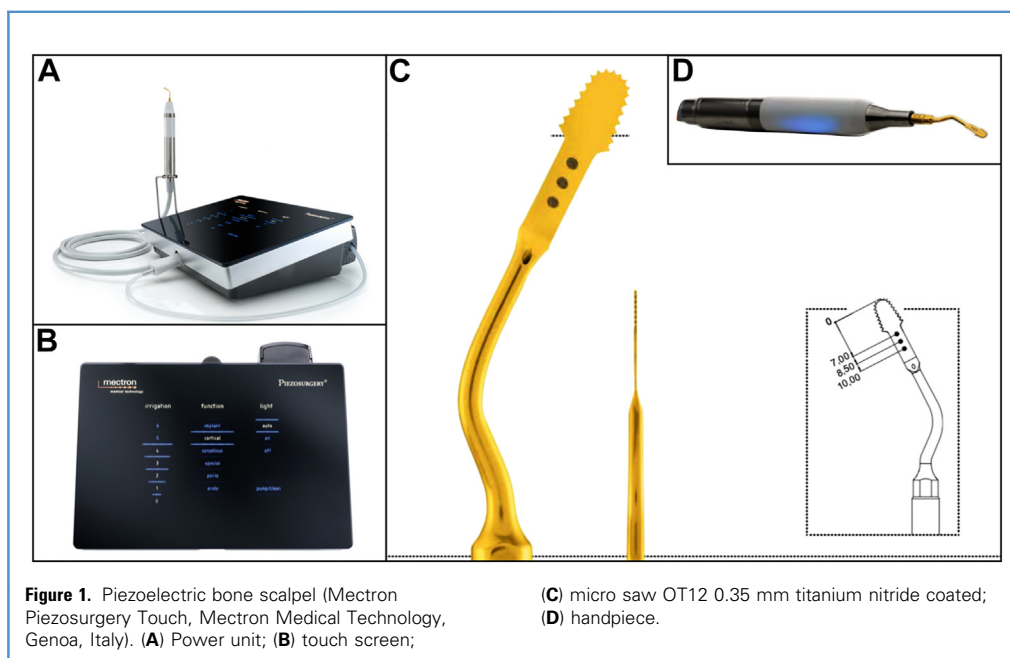


Figure 1. Piezoelectric bone scalpel (Mectron Piezosurgery Touch, Mectron Medical Technology, Genoa, Italy). (A) Power unit; (B) touch screen;

(C) micro saw OT12 0.35 mm titanium nitride coated; (D) handpiece.

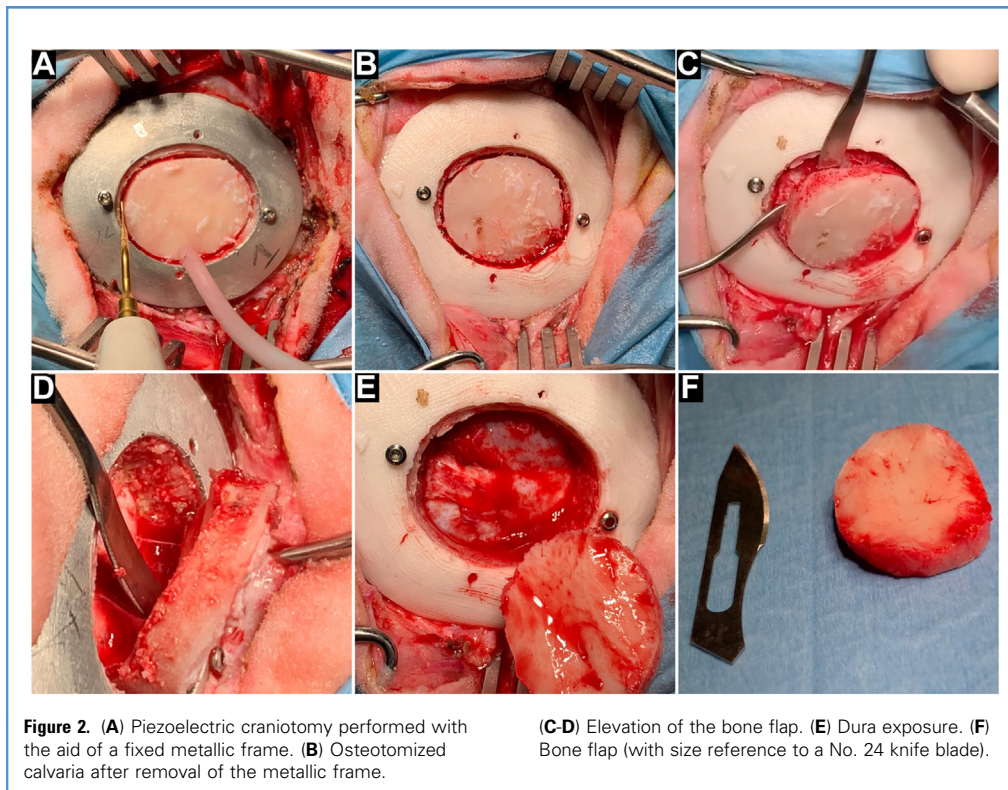


Figure 2. (A) Piezoelectric craniotomy performed with the aid of a fixed metallic frame. (B) Osteotomized calvaria after removal of the metallic frame.

(C-D) Elevation of the bone flap. (E) Dura exposure. (F) Bone flap (with size reference to a No. 24 knife blade).

Table 1. Histological Data			
Variable	Data		P Value
	Piezo Group	Control Group	
Total n° of Samples	21	19	
Site			
Cranial vault			
Smear layer evidence, n° (%)	2 (9.5)	16 (84.2)	<0.001*
Bone matrix evidence, n° (%)	16 (76.1)	6 (31.5)	0.003*
Osteoblast/HPF, mean ± SD	5.5 ± 3	3.1 ± 2	0.008*
Meninges			
Pachymeningeal injury, n° (%)	3 (14.2)	8 (42.1)	0.050
Leptomeningeal injury, n° (%)	1 (4.7)	8 (42.1)	0.003*
Cerebral parenchyma			
Gliosis evidence, n° (%)	2 (9.5)	7 (33.3)	0.039*
Histiocytic infiltration evidence, n° (%)	2 (9.5)	9 (47.3)	0.006*

HPF, high-power field; SD, standard deviation.
*Statistic.

cranial vault bone, while the dural sparing ability was determined by assessing the rate of pachymeningeal injury. Leptomeningeal injury, gliosis, and histiocytic infiltration were considered outcome measures of the aggressiveness of the instrument to the brain parenchyma.

Statistical Analysis

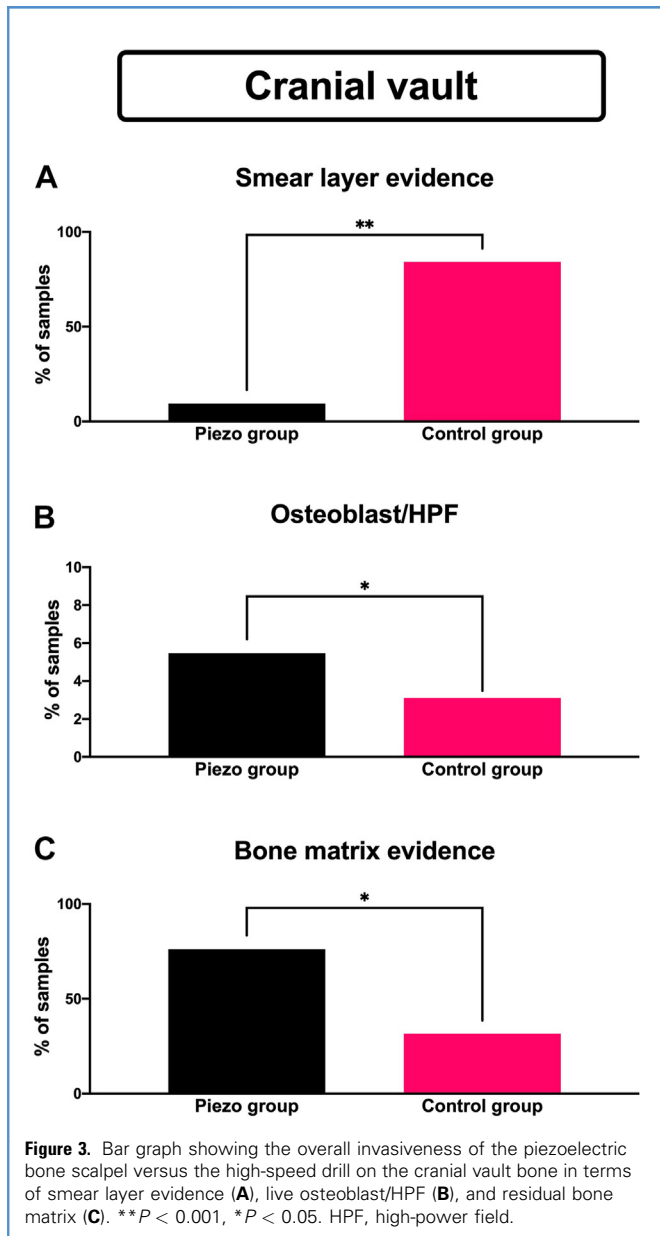
Categorical variables were reported as values and percentages, whereas continuous variables with normal distribution were expressed as means (\pm standard deviation).

Unpaired and Welch's t-tests were used for numerical and continuous variables, respectively. Prism 9 software (GraphPad Software, Inc., La Jolla, California, USA) was used for statistical analysis. A P value < 0.05 was considered significant.

RESULTS

In the Piezo group, the smear layer was less frequent ($P < 0.001$) and the residual amount of bone matrix was superior ($P < 0.05$). The mean number of live osteoblasts/high-power field was also greater ($P < 0.05$). The anatomical integrity of the pachymeninges was unaffected by either instrument type ($P > 0.05$), in contrast to the leptomeninges, which were more frequently injured in the control group ($P < 0.05$). The overall rate of cerebral gliosis and histiocytic infiltration was lower in the Piezo group ($P < 0.05$).

Table 1 summarizes the histologic data, and the bar graphs in Figures 3, 4, and 5 show the overall invasiveness of the

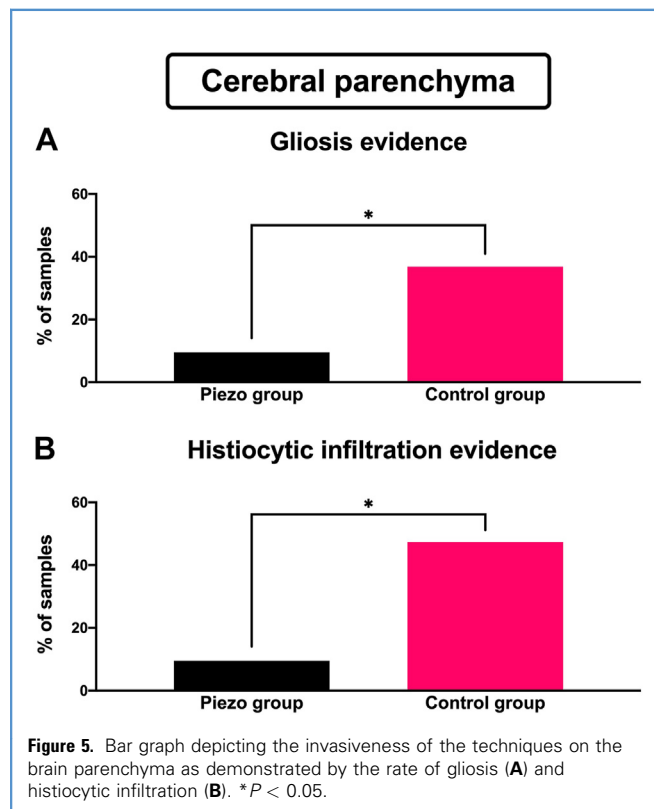
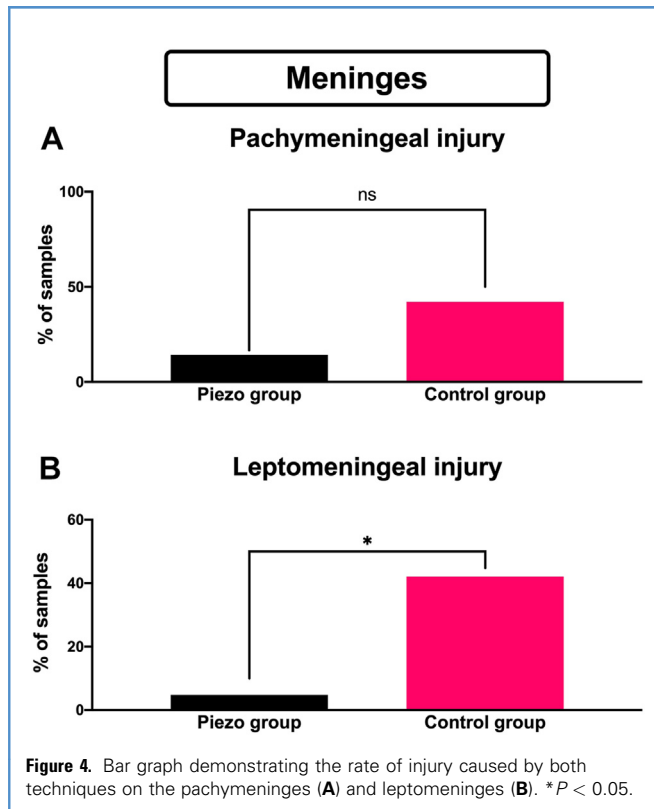


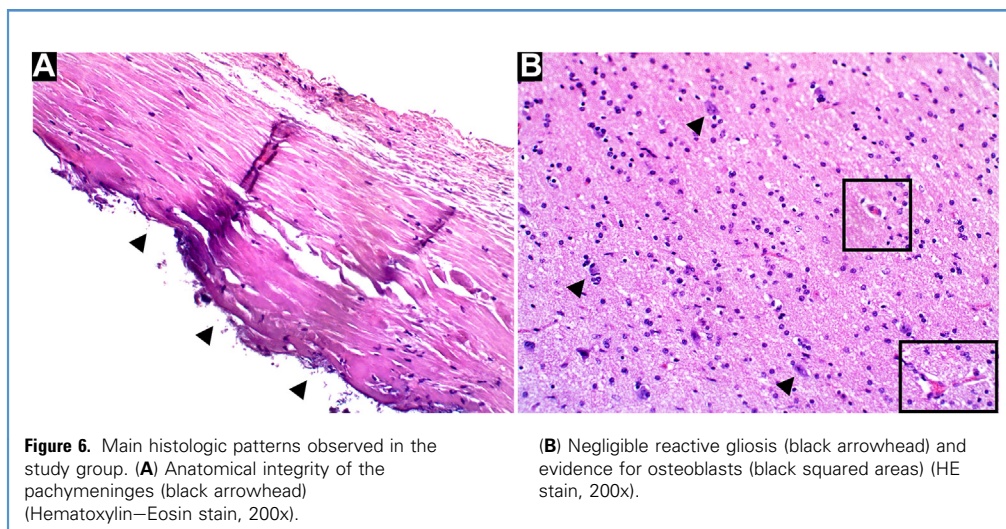
piezoelectric bone scalpel versus the high-speed drill on the cranial vault bone, meninges, and cerebral parenchyma, respectively.

Figures 6 and 7 show the major histologic patterns observed in the piezoelectric and control groups, respectively.

DISCUSSION

The present study evaluated the invasiveness of piezoelectric craniotomy from a histo-morphometric point of view while performing a comparative analysis with the high-speed drill in terms of physical and thermal iatrogenic damage to the adjacent cranial vault bone, meninges, and underlying brain tissue.

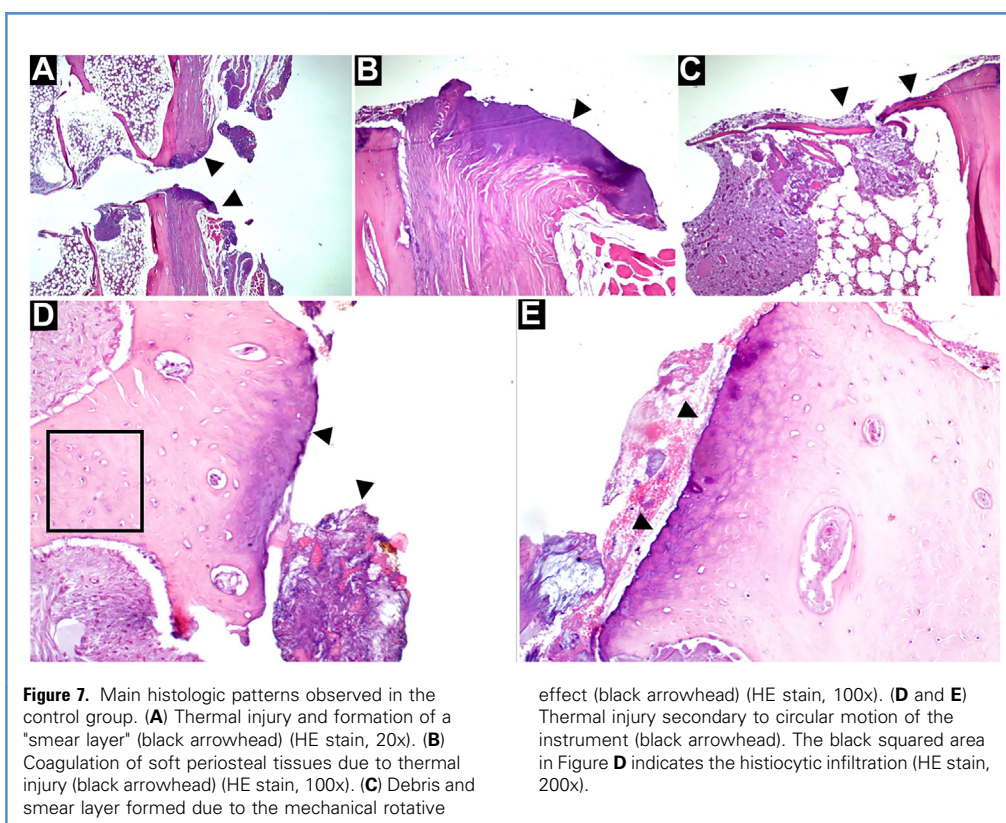




The piezoelectric bone scalpel proved to be less invasive than the drill for all outcome parameters except dural injury, which did not differ between groups. The reasons for these results may be that the average manual dexterity of the surgeons was sufficient to respect the anatomical integrity of the pachymeninges in both groups, but the thermal damage transmitted by the drill was

inherently higher. In support of this, the rate of thermally induced gliosis and histiocytic infiltration in the brain parenchyma was also significantly greater in the control group.

Piezosurgery has been reported to be less restrictive to bone healing than drills.³⁴⁻³⁷ This is due to its ability to stimulate bone morphogenetic proteins and bone remodeling while better



controlling iatrogenic inflammatory processes. Thinner bone gaps are another advantage. Preti et al.³⁷ reported a combined histomorphometric and molecular study of osseointegration after piezosurgical osteotomy in which fewer inflammatory cells, more osteoblasts, increased expression of bone morphogenetic proteins, and decreased expression of pro-inflammatory cytokines were observed.

The first histological description of postoperative bone healing dynamics dates back to 1975 by Horton et al.³⁶ They conducted an in vivo study on dog alveolar bone and found accelerated bone formation in alveolar defects. Similar data confirming the preserved viability of residual osteoblasts have been reported in ex vivo and in vivo studies in the field of oral surgery and implantology.^{37,35,38-40} However, there is still limited evidence on the histologic invasiveness of piezosurgery on the cranial vault.⁴¹⁻⁴⁴ Anesi et al.⁴¹ found a higher number of tartrate-resistant acid phosphatase-positive osteoclasts per linear surface in the piezo group compared to the rotating instruments in rabbit cranial osteotomies, indicating greater bone remodeling with the former. The main limitation of the rabbit skull is its limited surface area, which often prevents the performance of near-real craniotomies. Therefore, in the present study, the authors decided to use a larger model, such as the sheep.

As with rotating instruments, the cavitation phenomenon is known to be associated with an increase in local temperature.⁴⁵⁻⁴⁹ Two main factors affect the heat production of the piezoelectric scalpel, namely the load and the duration of the cut.

Stelzel et al. found that a harmful average temperature of $48.6 \pm 3.4^\circ\text{C}$ and a thermal effect of $200.7 \pm 44.4 \mu\text{m}$ are both achieved with a load between 900 and 1000 g, suggesting a maximum load of 400 g as safe.⁴⁸ Tepedino et al. found that the thermal wave of the piezoelectric scalpel remains below levels of clinical concern when the cutting time does not exceed 20 minutes.⁴⁵ Bone compactness has also been reported to play a role, as reported by Delgado-Ruiz et al.⁴⁶

The combination of these factors results in a site-specific probability of thermal damage that is higher in dense bone and lower in flat bones such as the skull, where the spongy component is also well represented. The less traumatic effect

on adjacent and underlying tissues that were found in the Piezo group could be explained by this dynamic. Similar data were reported by Rashad et al.,⁵⁰ who noted less heat generation with ultrasonic and sonic osteotomy systems compared to conventional saw osteotomy. Pavliková et al. also reported less depth and width of iatrogenic magnetic resonance imaging-detectable brain lesions in Wistar rats.⁵¹

Limitations of the Study

The present study has limitations, mainly due to its retrospective design, the relatively limited number of specimens, and the operator-dependent interpretation of most histologic data. The pressure load of the instrument should be considered as a potential source of bias in both groups. The authors fully recognize the importance of increasing the number of animal studies to further validate the findings of this research.

CONCLUSION

Piezoelectric craniotomy was shown to respect residual osteoblast viability and leptomeningeal integrity.

The lower rate of thermally induced gliosis and histiocytic infiltration demonstrated the minimal invasiveness of the piezoelectric osteotome to brain tissue compared to the high-speed drill.

Further evidence is needed to definitively validate these data before the use of the piezoelectric scalpel can be fully implemented in the neurosurgical scenario.

CRediT AUTHORSHIP CONTRIBUTION STATEMENT

Sabino Luzzi: Conceptualization, Data curation, Investigation, Software, Validation, Writing – original draft, Writing – review & editing. **Antonio Crovace:** Conceptualization, Supervision, Validation. **Sergio Carnevale:** Data curation, Formal analysis, Investigation, Methodology. **Luca Licitignola:** Investigation, Validation. **Francesco Staffieri:** Investigation, Validation. **Domenico Sfondrini:** Data curation, Investigation, Validation. **Edgar G. Ordóñez-Rubiano:** Data curation, Investigation, Validation. **Alberto Maria Crovace:** Conceptualization, Data curation, Investigation, Validation, Writing – original draft, Writing – review & editing.

REFERENCES

- Fukada E, Yasuda I. On the piezoelectric effect of bone. *J Phys Soc Jpn.* 1957;12:1158-1162.
- Schlee M, Steigmann M, Bratu E, Garg AK. Piezosurgery: basics and possibilities. *Implant Dent.* 2006;15:334-340.
- Brennen CE. *Cavitation and bubble dynamics.* Cambridge, UK: Cambridge university press; 2014.
- Eggers G, Klein J, Blank J, Hassfeld S. Piezosurgery®: an ultrasound device for cutting bone and its use and limitations in maxillofacial surgery. *Br J Oral Maxillofac Surg.* 2004;42:451-453.
- Leclercq P, Zenati C, Amr S, Dohan DM. Ultrasonic bone cut Part 1: state-of-the-art technologies and common applications. *J Oral Maxillofac Surg.* 2008;66:177-182.
- Marino A, Genchi GG, Sinibaldi E, Ciofani G. Piezoelectric effects of materials on bio-interfaces. *ACS Appl Mater Interfaces.* 2017;9:17663-17680.
- Yudin PV, Tagantsev AK. Fundamentals of flexoelectricity in solids. *Nanotechnology.* 2013;24:432001.
- Massimi L, Rapisarda A, Bianchi F, et al. Piezosurgery in pediatric neurosurgery. *World Neurosurg.* 2019;126:e625-e633.
- Vetrano IG, Prada F, Perin A, Casali C, DiMeco F, Saini M. Piezosurgery for infra- and supratentorial craniotomies in brain tumor surgery. *World Neurosurg.* 2019;122:e1398-e1404.
- Iacoangeli M, Rienzo AD, Nocchi N, et al. Piezosurgery as a further technical adjunct in minimally invasive supraorbital keyhole approach and lateral orbitotomy. *J Neurol Surg Cent Eur Neurosurg.* 2015;76:112-118.
- Salami A, Dellepiane M, Mora R. A novel approach to facial nerve decompression: use of piezosurgery. *Acta Otolaryngol.* 2008;128:530-533.
- Salami A, Dellepiane M, Proto E, Mora R. Piezosurgery in otologic surgery: four years of experience. *Otolaryngol Head Neck Surg.* 2009;140:412-418.
- Salami A, Mora R, Mora F, Guastini L, Salzano FA, Dellepiane M. Learning curve for piezosurgery in well-trained otological surgeons. *Otolaryngol Head Neck Surg.* 2010;142:120-125.
- Salami A, Vercellotti T, Mora R, Dellepiane M. Piezoelectric bone surgery in otologic surgery. *Otolaryngol Head Neck Surg.* 2007;136:484-485.
- Franzini A, Legnani F, Beretta E, et al. Piezoelectric surgery for dorsal spine. *World Neurosurg.* 2018;114:58-62.

16. Ramieri V, Saponaro G, Lenzi J, et al. The use of piezosurgery in cranial surgery in children. *J Craniofac Surg.* 2015;26:840-842.
17. Martini M, Röhrig A, Reich RH, Messing-Jünger M. Comparison between piezosurgery and conventional osteotomy in cranioplasty with fronto-orbital advancement. *J Cranio-Maxillofacial Surg.* 2017;45:395-400.
18. Kotrikova B, Wirtz R, Krempien R, et al. Piezosurgery—a new safe technique in cranial osteoplasty? *Int J Oral Maxillofac Surg.* 2006;35:461-465.
19. Acharya AN, Rajan GP. Piezosurgery for the repair of middle cranial fossa meningoencephaloceles. *Otol Neurotol.* 2015;36:444-447.
20. Jung SH, Ferrer AD, Vela JS, Granados FA. Spheno-orbital meningioma resection and reconstruction: the role of piezosurgery and premolded titanium mesh. *Cranio-Maxillofac Trauma Reconstr.* 2011;4:193-200.
21. Grauvogel J, Scheiwe C, Kaminsky J. Use of piezosurgery for internal auditory canal drilling in acoustic neuroma surgery. *Acta Neurochir (Wien).* 2011;153:1941-1947.
22. Grauvogel J, Masalha W, Heiland DH, Jarc N, Grauvogel TD, Scheiwe C. Piezosurgery—a safe technique to perform lateral suboccipital craniotomy? *Oper Neurosurg (Hagerstown).* 2017;15:664-671.
23. Schaller BJ, Gruber R, Merten HA, et al. Piezoelectric bone surgery: a revolutionary technique for minimally invasive surgery in cranial base and spinal surgery? Technical note. *Neurosurgery.* 2005;57(4 Suppl):E410 [discussion: E410].
24. Crovace AM, Luzzi S, Lacitignola L, et al. Minimal invasive piezoelectric osteotomy in neurosurgery: technic, applications, and clinical outcomes of a retrospective case series. *Vet Sci.* 2020;7:68.
25. Grauvogel J, Scheiwe C, Kaminsky J. Use of Piezosurgery for removal of retrovertebral body osteophytes in anterior cervical discectomy. *Spine J.* 2014;14:628-636.
26. Pan SF, Sun Y. Application of piezosurgery in anterior cervical corpectomy and fusion. *Orthop Surg.* 2016;8:257-259.
27. Vercellotti T. Technological characteristics and clinical indications of piezoelectric bone surgery. *Minerva Stomatol.* 2004;53:207-214.
28. Vercellotti T, Nevins ML, Kim DM, et al. Osseous response following resective therapy with piezosurgery. *Int J Periodontics Restor Dent.* 2005;25:543-549.
29. Sanborn MR, Balzer J, Gerszten PC, Karausky P, Cheng BC, Welch WC. Safety and efficacy of a novel ultrasonic osteotome device in an ovine model. *J Clin Neurosci.* 2011;18:1528-1533.
30. Giraud JY, Villemin S, Darmana R, Cahuzac JP, Autefage A, Morucci JP. Bone cutting. *Clin Phys Physiol Meas.* 1991;12:1-19.
31. Tehemar SH. Factors affecting heat generation during implant site preparation: a review of biologic observations and future considerations. *Int J Oral Maxillofac Implants.* 1999;14:127-136.
32. Chacon GE, Bower DL, Larsen PE, McGlumphy EA, Beck FM. Heat production by 3 implant drill systems after repeated drilling and sterilization. *J Oral Maxillofac Surg.* 2006;64:265-269.
33. Queiroz TP, Souza FÁ, Okamoto R, et al. Evaluation of immediate bone-cell viability and of drill wear after implant osteotomies: immunohistochemistry and scanning electron microscopy analysis. *J Oral Maxillofac Surg.* 2008;66:1233-1240.
34. Chiriac G, Herten M, Schwarz F, Rothamel D, Becker J. Autogenous bone chips: influence of a new piezoelectric device (Piezosurgery) on chip morphology, cell viability and differentiation. *J Clin Periodontol.* 2005;32:994-999.
35. Happe A. Use of a piezoelectric surgical device to harvest bone grafts from the mandibular ramus: report of 40 cases. *Int J Periodontics Restor Dent.* 2007;27:241-249.
36. Horton JE, Tarpley Jr TM, Wood LD. The healing of surgical defects in alveolar bone produced with ultrasonic instrumentation, chisel, and rotary bur. *Oral Surg Oral Med Oral Pathol.* 1975;39:536-546.
37. Preti G, Martinasso G, Peirone B, et al. Cytokines and growth factors involved in the osseointegration of oral titanium implants positioned using piezoelectric bone surgery versus a drill technique: a pilot study in minipigs. *J Periodontol.* 2007;78:716-722.
38. Sohn DS, Ahn MR, Lee WH, Yeo DS, Lim SY. Piezoelectric osteotomy for intraoral harvesting of bone blocks. *Int J Periodontics Restor Dent.* 2007;27:127-131.
39. Heinemann F, Hasan I, Kunert-Keil C, et al. Experimental and histological investigations of the bone using two different Oscillating Osteotomy techniques compared with conventional rotary osteotomy. *Ann Anat.* 2012;194:165-170.
40. Ma L, Stübinger S, Liu XL, Schneider UA, Lang NP. Healing of osteotomy sites applying either piezosurgery or two conventional saw blades: a pilot study in rabbits. *Int Orthop.* 2013;37:1597-1603.
41. Anesi A, Ferretti M, Cavani F, et al. Structural and ultrastructural analyses of bone regeneration in rabbit cranial osteotomy: piezosurgery versus traditional osteotomes. *J Cranio-Maxillo-Fac Surg.* 2018;46:107-118.
42. Maurer P, Kriwalsky MS, Block Veras R, Vogel J, Syrowatka F, Heiss C. Micromorphometrical analysis of conventional osteotomy techniques and ultrasonic osteotomy at the rabbit skull. *Clin Oral Implants Res.* 2008;19:570-575.
43. Hollstein S, Hoffmann E, Vogel J, Heyroth F, Prochnow N, Maurer P. Micromorphometrical analyses of five different ultrasonic osteotomy devices at the rabbit skull. *Clin Oral Implants Res.* 2012;23:713-718.
44. Yang BE, Girod S. Efficacy of bone healing in calvarial defects using piezoelectric surgical instruments. *J Craniofac Surg.* 2014;25:149-153.
45. Tepedino M, Romano F, Indolfi M, Aimetti M. Heat production and drill wear following osseous resective surgery: a preliminary in vitro sem study comparing piezosurgery and conventional drilling. *Int J Periodontics Restor Dent.* 2018;38:e33-e40.
46. Delgado-Ruiz RA, Sacks D, Palermo A, Calvo-Guirado JL, Perez-Albacete C, Romanos GE. Temperature and time variations during osteotomies performed with different piezosurgical devices: an in vitro study. *Clin Oral Implants Res.* 2016;27:1137-1143.
47. Noetzel N, Fienitz T, Kreppel M, Zirk M, Safi AF, Rothamel D. Osteotomy speed, heat development, and bone structure influence by various piezoelectric systems-an in vitro study. *Clin Oral Investig.* 2019;23:4029-4041.
48. Stelzle F, Frenkel C, Riemann M, Knipfer C, Stockmann P, Nkenke E. The effect of load on heat production, thermal effects and expenditure of time during implant site preparation - an experimental ex vivo comparison between piezosurgery and conventional drilling. *Clin Oral Implants Res.* 2014;25:e140-e148.
49. Bhargava N, Perrotti V, Caponio VCA, Matsubara VH, Patalwala D, Quaranta A. Comparison of heat production and bone architecture changes in the implant site preparation with compressive osteotomes, osseodensification technique, piezoelectric devices, and standard drills: an ex vivo study on porcine ribs. *Odontology.* 2023;111:142-153.
50. Rashad A, Sadr-Eshkevari P, Heiland M, et al. Intraosseous heat generation during sonic, ultrasonic and conventional osteotomy. *J Cranio-Maxillo-Fac Surg.* 2015;43:1072-1077.
51. Pavlíková G, Foltán R, Burian M, et al. Piezosurgery prevents brain tissue damage: an experimental study on a new rat model. *Int J Oral Maxillofac Surg.* 2011;40:840-844.

Conflict of interest statement: The authors declare that the article content was composed in the absence of any commercial or financial relationships that could be construed as a potential conflict of interest.

Received 15 August 2024; accepted 17 August 2024

Citation: *World Neurosurg.* (2024) 191:e160-e166.

<https://doi.org/10.1016/j.wneu.2024.08.088>

Journal homepage: www.journals.elsevier.com/world-neurosurgery

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